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2

3 **Title:** Perceptual and objective physical quality of chest images: a comparison between digital
4 radiographic chest images processed for cancer screening and pneumoconiosis screening in
5 Japan

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25 **Running title:** PROCESSING PARAMETERS AND QUALITY OF CHEST IMAGES

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31 **Abstract:** This study (1) evaluated the perceptual and objective physical quality of digital
32 radiographic chest images processed for different purposes (routine hospital use, lung cancer
33 screening, and pneumoconiosis screening), and (2) quantified objectively the quality of chest
34 images visually graded by the Japan National Federation of Industrial Health Organization
35 (ZENEIREN). Four observers rated the images using a visual grading score (VGS) according to
36 ZENEIREN's quality criteria. Signal-to-noise ratio (SNR) and contrast-to-noise ratio (CNR)
37 were measured. Between groups, differences were assessed using ANOVA (followed by
38 Bonferroni multiple comparisons) or unpaired t-test. The Pearson's correlation coefficients were
39 calculated for the correlation between perceptual quality and objective physical image quality.
40 The image quality perceived by the observers and the SNR measurements were highest for the
41 images generated using parameters recommended for lung cancer screening. The images
42 processed for pneumoconiosis screening were rated poorest by the observers and showed the
43 lowest objective physical quality measurements. The chest images rated high quality by
44 ZENEIREN generally showed a higher objective physical image quality. The SNR correlated
45 well with VGS, but CNR did not. Highly significant differences between the processing
46 parameters indicate that image processing strongly influences the perceptual quality of digital
47 radiographic chest images.

48

49 **Keywords:** Chest radiography, Contrast-to-noise ratio, Quality control, Signal-to-noise ratio,
50 Visual grading analysis, X-Rays

51

52 INTRODUCTION

53 Chest radiography is one of the most frequently performed radiographic examinations in
54 routine clinical diagnosis and health screening worldwide. Digital image acquisition and
55 processing techniques can enhance the diagnostic image quality by improving contrast and
56 spatial resolution, and by reducing noise¹⁾. Parameters for image processing differ depending on
57 the targeted anatomical and pathological structures and the radiologists' preference. In Japan, it
58 is recommended that digital radiographic chest images for lung cancer screening be processed
59 using parameters such as multi-frequency processing and dynamic range compression²⁾. These
60 parameters were designed for better visualization of images and enable demonstration of certain
61 pathological lesions more clearly. However, for pneumoconiosis screening, the Japanese
62 Ministry of Health, Labour and Welfare (MHLW) recommends processing parameters that
63 appear to produce an image similar to the film-screen radiograph^{3,4)}. The setting uses almost no
64 processing applicable to the digital image; for example, greyscale processing of the mediastinum
65 is omitted, spatial frequency processing is off, and multi-frequency processing that enables
66 differential processing at the areas with high and low frequencies also is not applied^{3,4)}.
67 Therefore, the images produced for the two screening purposes might differ in perceptual and
68 objective physical quality. However, no reports have evaluated the quality of these images.

69 In Japan, general health check-ups and medical screening in workplaces are typically
70 provided by health check-up facilities, public and private hospitals, and health facilities owned
71 by large-scale enterprises. Good quality chest imaging is essential to accurate diagnosis of
72 pulmonary disease. To maintain the quality of chest images, the Japan National Federation of
73 Industrial Health Organization (ZENEIREN) has since 1980 offered an annual quality assurance
74 program²⁾. The designated quality assurance committee evaluates the image quality using a

75 visual grading analysis according to the quality criteria developed by ZENEIREN. Images are
76 assessed for clinical quality (visibility of anatomical structures) and technical quality
77 (satisfactory level of contrast, exposure, sharpness, and graininess) and are assigned a visual
78 grading score (VGS). Three hundred fifty medical facilities submitted a total of 1,050 images in
79 2019. Image quality can be determined subjectively by performing a visual assessment or
80 objectively by measuring physical parameters (such as signal-to-noise ratio [SNR] and contrast-
81 to-noise ratio [CNR])⁵). The visual assessment method used by ZENEIREN requires predefined
82 quality criteria and experts' evaluation; the grading reflects the image quality perceived by the
83 experts and has potential for variation. On the other hand, measuring SNR or CNR is relatively
84 simple, easy to perform, and consistent. However, we found no study, at least in the English
85 language literature, that has objectively evaluated the quality of chest images visually assessed
86 and graded by ZENEIREN.

87 For the reasons mentioned above, we conducted the present study. Firstly, we compared
88 the perceptual and objective physical quality of clinical chest images produced using different
89 processing parameters. Secondly, we evaluated whether objective physical quality assessment
90 (by measuring SNR or CNR) was appropriate as an alternative method to the visual grading
91 analysis used by ZENEIREN.

92

93 **SUBJECTS AND METHODS**

94 We obtained prior approval from Kochi Medical School and ZENEIREN for chest
95 images used in this study. Since this study used only anonymized images, written informed
96 consent from the patients was waived. The study protocol was approved by the institutional

97 review board of Kochi Medical School. Image quality was evaluated using a visual grading
98 analysis⁶⁾ and objective physical measurements.

99

100 *Images acquisition*

101 This study used two sets of chest images. Set 1 included 30 chest images with no
102 abnormal shadow taken from thirty patients between August and October 2017 at Kochi Medical
103 School Hospital. Set 2 included a total of 12 images (6 high-quality images and 6 low-quality
104 images graded by ZENEIREN) randomly selected from the images submitted to ZENEIREN
105 from various medical facilities for quality assessment in 2014 and 2016. We re-developed every
106 image in set 1 (30 images) using three different processing parameters: (1) parameters
107 recommended by ZENEIREN for lung cancer screening (Ca-parameter)²⁾; (2) parameters
108 recommended by the MHLW for pneumoconiosis screening (P-parameter)^{3, 4)}; and (3)
109 parameters used clinically at Kochi Medical School Hospital (generally, routine hospital chest
110 images are aiming to detect lung cancer) (H-parameter) (Table 1). The resulting set of 90 chest
111 images was used in the analyses to evaluate the quality of images produced using different
112 processing parameters.

113 Set 1 images were acquired using MRAD-A80S RADREX (High voltage unit: KXO-
114 80SS, X-ray tube: DRX-4634HC) general X-ray system (CANON MEDICAL SYSTEMS
115 CORPORATION, Ohtawara, Tochigi, Japan), We also used CALNEO Smart DR-ID1200
116 Digital radiography (DR) system (FPD: CALNEO Smart C77 DR-ID 1212SE, workstation:
117 Console Advance DR-ID 300CL) (FUJIFILM, Minato, Tokyo, Japan), FM-PU1 digital bucky
118 stand (OBAYASHI MFG.CO., LTD, Bunkyo, Tokyo, Japan) and anti-scatter grid (strips per
119 centimetre: 40, grid ratio:12/1, focusing distance: 200cm, interspace material: aluminium)

120 (MITAYA MFG.CO., LTD, Kawagoe, Saitama, Japan). We set focus-FPD distance 200cm, X-
121 ray tube voltage was 120kV, tube current was 320mA, photographing time set auto exposure
122 control (AEC), and set the 1.5mmAl+0.1mmCu filter.

123 (insert Table 1)

124

125 *Assessment of perceptual image quality*

126 Four experienced observers, who were blinded to the processing parameters,
127 independently assessed the set of 90 images on a diagnostic monitor (5-megapixel [2,048 X
128 2,560 pixels]) using a DICOM-Viewer. The illumination in the room was dim and kept constant.
129 There was no limitation concerning viewing time or viewing distance. The assessment was made
130 for both clinical and physical image quality using absolute visual grading analysis according to
131 ZENEIREN's quality criteria²⁾. Clinical image quality was determined by the visibility of
132 anatomical structures. These include skeletal structures (clavicles, ribs, thoracic vertebrae),
133 mediastinal structures (heart shadow and pulmonary arteries), tracheobronchial and pulmonary
134 parenchymal structures (lung margin, vascular markings of lung zones). Physical quality was
135 determined by satisfactory levels in the contrast, exposure, sharpness, and graininess of the
136 images. Two observers, an occupational physician with over twenty years of experience (who is
137 a NIOSH certified B Reader and also a member of ZENEIREN's quality assurance committee)
138 and a radiologist with six years of experience in general radiology, assessed and provided the
139 clinical image quality aspect of VGS (total 70 points). Two radiologic technologists with more
140 than eight years of working experience assessed and provided the physical image quality aspect
141 of VGS (total 30 points). Combining the assessment results for both quality aspects gave a total
142 score of 100 points. Before starting the assessment, the observer who is a member of

143 ZENEIREN's quality assurance committee explained the quality assessment criteria of
144 ZENEIREN. Every image was assessed and graded accordingly as "A" (excellent quality, 85–
145 100 points; overall abnormalities can be recognized easily), "B" (good quality, 70–84 points; not
146 the quality of grade "A" but abnormalities can still be recognized easily), "C" (fair quality, 60–
147 69 points; possible/adequate for routine diagnostic radiography), and "D" (poor quality, <60
148 points; not suitable for routine diagnostic radiography).

149

150 *Assessment of objective physical image quality*

151 We selected the regions of interest (ROIs) based on the image's fields defined by
152 ZENEIREN in the quality evaluation of chest images²⁾. To calculate SNR, we established two
153 rectangle-shaped ROIs (ROI-I and ROI-II) and one right lung field ROI (ROI-III) (Fig. 1a). The
154 ROI-I covers both sides of the chest and contains heart shadow, while the ROI-II encloses the
155 right half of the chest, including a part of heart shadow and mediastinum, and the ROI-III
156 includes only the right lung field. Measurement of CNR was carried out using four pairs of
157 ROIs: ROI-1, 7th thoracic vertebral body and right 6th–7th intercostal lung field; ROI-2, left
158 10th–11th intercostal cardiac shadow and left lower lobe lung field; ROI-3, right middle
159 diaphragm and right lower lobe lung field; and ROI-4, the soft tissue of right shoulder and right
160 4th–5th intercostal lung field (Fig. 1b). We measured the mean values and standard deviation
161 (SD) of all the pixels contained within the selected ROI of the images by using an open-source
162 image processing program ImageJ ver.1.49v⁷⁾. The image noise level was defined by the SD of
163 the pixels in the selected ROI. We computed the SNR and CNR using the following equations:
164 $SNR (ROI) = \text{Mean signal (ROI)} / SD (ROI)$; and $CNR = [\text{Mean signal (tissue)} - \text{Mean signal}$

165 (lung field)]/ SD (ROI-5). ROI-5 covers both sides of the chest as in ROI-I of SNR
166 measurement.

167

168 (insert Fig. 1)

169

170 *Statistical analysis*

171 Mean scores of VGS, SNR, and CNR were used to assess the differences in the
172 perceptual and objective physical quality of images due to differences in image processing
173 parameters. The significance of differences was determined using one-way analysis of variance
174 followed by Bonferroni multiple comparisons. Correlation between the perceptual (VGS) and
175 objective physical (SNR and CNR) image quality was determined by Pearson's correlation
176 coefficient. To examine whether the objective physical quality assessment was appropriate as an
177 alternative method to the visual grading analysis, we measured the SNR and CNR of high- and
178 low-quality images (graded by the ZENEIREN) and compared their mean values using unpaired
179 t-test. A p -value of <0.05 was considered statistically significant. All statistical analyses were
180 performed using Microsoft Excel for Windows.

181

182 **RESULTS**

183 Tables 2–4 compare the mean VGS, SNR, and CNR between images produced using different
184 processing parameters. Mean VGS for both the clinical quality and technical quality of images
185 processed using the Ca-parameter were significantly higher than those images processed using P-
186 parameter and H-parameter (Table 2). Differences in VGS were mainly found in subcategory
187 scores for visibility in skeletal structures (particularly thoracic vertebrae) and pulmonary

188 parenchymal structures (particularly lung margin under diaphragm and vascular markings of
189 lung zones) in clinical quality assessment and contrast, mediastinal density, and sharpness in
190 technical quality assessment (data not shown). A significantly higher mean SNR was also found
191 for images processed using Ca-parameter (Table 3), whereas no difference in the mean CNR was
192 observed between images developed by different processing parameters (Table 4).

193 (insert Table 2, Table 3, and Table 4)

194 Figures 2 and 3 show the correlation between perceptual quality (VGS) and objective physical
195 quality (SNR and CNR) of the images. Correlation between VGS and SNR was stronger in ROI-
196 I ($r = 0.77, p < 0.01$) and in ROI-II ($r = 0.76, p < 0.01$) than that seen in ROI-III ($r = 0.40, p =$
197 0.01) (Fig. 2). Pearson's correlation coefficients between VGS and CNR were -0.16, 0.35, 0.15
198 and -0.01, for ROI-1, ROI-2, ROI-3 and ROI-4, respectively (Fig. 3).

199 (insert Fig. 2 and Fig. 3)

200 Table 5 presents the mean SNR and CNR for high-quality and low-quality images visually
201 graded by ZENEIREN. When compared with low-quality, high-quality images show
202 significantly higher mean SNR in ROI-I and ROI-II ($p < 0.001$) and higher mean CNR in ROI-4
203 ($p < 0.05$) (Table 5).

204 (insert Table 5)

205

206 **DISCUSSION**

207 In the present study, we attempted to compare the quality of chest images generated using
208 different processing parameters and found significant differences. We found that the image
209 processing parameter used for cancer screening produces significantly higher quality chest
210 images than the parameters for routine hospital chest images and pneumoconiosis screening in

211 Japan. We also observed that SNR showed a strong positive correlation with perceived image
212 quality, whereas CNR showed a poor correlation. Moreover, chest images rated high-quality by
213 ZENEIREN were generally found to have higher objective physical quality.

214 We found image processing had a significant effect on the quality of digital radiographic
215 chest images. One African study also reported that visibility of the object and objective physical
216 quality (SNR and CNR) were different with different processing parameters⁸⁾. However, in a
217 recent study, Smet et al.⁹⁾ found no effect of image processing on perceived image quality,
218 measured by the visibility of anatomical structures. The discrepancy among studies might be due
219 to the differences in the processing parameters studied (the use of manufacturer-specific
220 processing software or pathology-specific processing parameters) or the evaluation methods
221 (object detection or visibility of anatomical structures). In the present study, the image quality
222 perceived by the observers was highest for the images processed using parameters recommended
223 for lung cancer screening, and the SNR also reflected the perceptual image quality. The images
224 processed using parameters recommended for pneumoconiosis screening were rated poorest by
225 the observers and showed the lowest objective physical quality measurements. The main
226 differences between processing parameters used in our study are the presence or absence and the
227 degree of dynamic range compression and multi-frequency processing. As seen in Table 1,
228 image processing for lung cancer screening applied these techniques, whereas image processing
229 for pneumoconiosis screening omitted or used them to a lower degree. These processing
230 techniques provide the potential to improve image quality¹⁰⁾. Multi-frequency processing
231 decomposes the image into a series of sub-frequency images and reconstructs them back into a
232 single image with optimized contrast. Dynamic range compression allows viewing detail behind
233 the heart and diaphragm while retaining the greyscale and detail of the lung field. Therefore, in

234 the present study, images processed using these techniques received a higher appreciation of
235 image quality by the observers.

236 In the present study, we observed a good correlation between SNR and perceived image
237 quality, and this finding was consistent with other past studies^{11, 12}). Image quality assessment
238 using visual grading analysis involves observers considering how much image detail (i.e., the
239 anatomical structures or abnormalities) they could see. In digital chest images, the noise would
240 possibly hinder the visualization of subtle anatomical structures and pathological lesions. Thus,
241 improving SNR would enhance perceived image quality. We found the correlation between VGS
242 and CNR was poor and inconsistent. However, Moore et al. reported a significant correlation
243 between VGS and CNR¹³). This discrepancy might originate from differences in the study
244 design. In their study, Moore et al. tested the correlation between VGS (scored using chest
245 images) and CNR (measured using chest phantom); however, we used the same chest images for
246 both subjective and objective quality assessments. In addition, they generated images by
247 changing tube voltages, whereas we generated them using different processing parameters. Huda
248 and Abrahams described that although a high lesion contrast improves diagnostic quality, it is
249 not important for perceived image quality¹⁴). We suggest that, in some cases, an increase in the
250 density of soft tissue shadows such as the heart may hinder visualization of the anatomical
251 structure behind it. In quality evaluation, the evaluators of ZENEIREN assess several specified
252 regions of the images, combine the scores, and determine image quality using quality criteria.
253 The use of the overall VGS score in our study might be the reason for the observed reduced
254 correlation with SNR measurement in ROI-III (which includes only the right lung field) and the
255 poor correlation with CNR measurements in all ROIs. In a study, Lin and coworkers have
256 demonstrated a significant correlation between physical quality measurements and perceptual

257 quality of clinical chest radiographs¹⁵). In their study, the authors specified several ROIs; then
258 examined the correlation of quantitative quality measurement of a region with the corresponding
259 perceptual evaluation.

260 Chest images rated high-quality by ZENEIREN generally have higher objectively-
261 measured physical image quality. However, significant differences between the low-quality and
262 high-quality images were observed only for SNR measurements performed in ROI-I and ROI-II
263 and CNR measurement in ROI-4. We suggest that the correlation observed between perceived
264 image quality (VGS) and objective quality measurements (SNR and CNR) and the choice of ROI
265 for measuring SNR and CNR might be the possible explanations. We found the correlation
266 between VGS and SNR was stronger when SNR measurement contained the whole (ROI-I) or
267 half (ROI-II) of the cardiac shadow, mediastinal structures, and thoracic vertebrae. However, the
268 correlation attenuated when the SNR measurement included only the right lung field (ROI-III).
269 In digital chest images, structures such as the heart, mediastinum, thoracic vertebrae, and
270 diaphragm can negatively affect the visibility of subtle anatomical structures, and consequently,
271 the observer's perception of image quality. These anatomical structures also influence the image's
272 noise level, and subsequently, SNR. Thus, SNR measurements that include these anatomical
273 structures (ROI-I and ROI-II) better reflect the VGS. We also observed that the mean SNR
274 values of Set 1 images were higher than those of Set 2 images. A potential reason for the
275 observed difference may be that the images in Set 2 were generated using different modalities or
276 manufacturer-specific processing software, because they were submitted to ZENEIREN from
277 various medical facilities.

278 The Pneumoconiosis law of Japan requires screening and legal judgements of
279 pneumoconiosis to be performed using a chest radiograph. However, the application of multi-

280 frequency processing or dynamic range control is not fully allowed in image processing. These
281 parameters were designed for better visualization of digital chest images, and we found using
282 them received a higher appreciation of image quality by the observers. Although we did not
283 investigate it, we suggest these parameters may enable the demonstration of pneumoconiosis
284 more clearly. Since over- or under-classifying pneumoconiosis severity imposes substantial
285 social and economic costs, we recommend further research to evaluate adequacy in classifying
286 chest images for pneumoconiosis (using the classification system specified by the
287 Pneumoconiosis law of Japan) using images processed with different parameter settings,
288 including the one recommended by ZENEIREN. Among the strengths of this study are that it is
289 the first to compare the quality of chest images generated using different processing parameters
290 for different purposes in Japan. The quality evaluation was performed using clinical chest images
291 according to ZENEIREN's quality criteria. One potential limitation of this study is the small
292 number of chest images evaluated by ZENEIREN, which we used for the objective image quality
293 quantification. In recent years, the number of digital chest images graded poor-quality by
294 ZENEIREN has been on the decline. However, we believe that the inclusion of more images
295 would not substantially change the results.

296

297 **CONCLUSION**

298 This study demonstrates that the parameters used to process lung cancer screening images
299 in Japan produce significantly better quality images than those used to process pneumoconiosis
300 screening images. However, at present, we cannot conclude that the chest images for lung cancer
301 screening are better at detecting or classifying pneumoconiosis severity. Further investigation
302 evaluating the diagnostic ability as well as the adequacy in classifying pneumoconiosis severity

303 of these images is needed. A strong correlation between SNR and perceived image quality
304 suggests that measuring SNR could be an alternative to visual grading analysis when expert
305 judgment is not readily available. However, the perceptual quality of chest images cannot be
306 predicted from the measurement of CNR alone.

307

308

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373

374 **Figure legends**

375 **Fig 1.** Illustration of the regions of interest (ROIs). **(a)** Measurement of signal-to-noise ratio:
376 ROI-I, both sides of the chest; ROI-II, right half of the chest; ROI-III, right lung field; **(b)**
377 Measurement of contrast-to-noise ratio: ROI-1, 7th thoracic vertebral body and right 6th–7th
378 intercostal lung field; ROI-2, left 10th–11th intercostal cardiac shadow and left lower lobe lung
379 field; ROI-3, right middle diaphragm and right lower lobe lung field; and ROI-4, soft tissue of
380 right shoulder and right 4th–5th intercostal lung field.

381

382 **Fig 2.** Correlation between visual grading score and signal-to-noise ratio (SNR) in **(a)** ROI-I, **(b)**
383 ROI-II, and **(c)** ROI-III. ROI, region of interest: ROI-I, both sides of the chest; ROI-II, right half
384 of the chest; ROI-III, right lung field. r , Pearson's correlation coefficients; Ca-parameter,
385 parameters recommended by ZENEIREN for lung cancer screening; P-parameter, parameters
386 recommended by Japanese Ministry of Health, Labour and Welfare for pneumoconiosis
387 screening; and H-parameter, parameters used clinically at Kochi Medical School Hospital for
388 routine chest images.

389

390 **Fig 3.** Correlation between visual grading score and contrast-to-noise ratio (CNR) in **(a)** ROI-1,
391 **(b)** ROI-2, **(c)** ROI-3, and **(d)** ROI-4. ROI, region of interest: ROI-1, 7th thoracic vertebral body
392 and right 6th–7th intercostal lung field; ROI-2, left 10th–11th intercostal cardiac shadow and left
393 lower lobe lung field; ROI-3, right middle diaphragm and right lower lobe lung field; and ROI-4,
394 soft tissue of right shoulder and right 4th–5th intercostal lung field. r , Pearson's correlation
395 coefficients; Ca-parameter, parameters recommended by ZENEIREN for lung cancer screening;
396 P-parameter, parameters recommended by Japanese Ministry of Health, Labour and Welfare for

397 pneumoconiosis screening; and H-parameter, parameters used clinically at Kochi Medical

398 School Hospital for routine chest images.

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